

Radboud University



Introduction to EEG, MEG and analysis with the FieldTrip toolbox

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What is FieldTrip

a MATLAB toolbox for the analysis of MEG, EEG and animal electrophysiology data

can import data from many different file formats

contains algorithms for spectral analysis, source reconstruction, statistics, connectivity, ...

Talk outline

What kind of signals are generated in the brain

How do we record those signals

Analyzing those signals with FieldTrip

Background on the FieldTrip toolbox

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What kind of signals are generated in the brain

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Analyzing those signals with FieldTrip

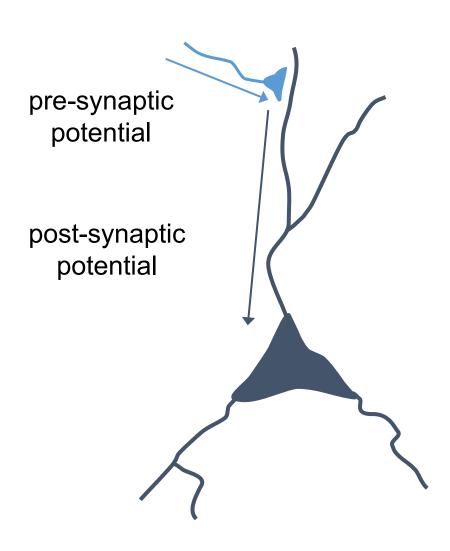
Background on the FieldTrip toolbox

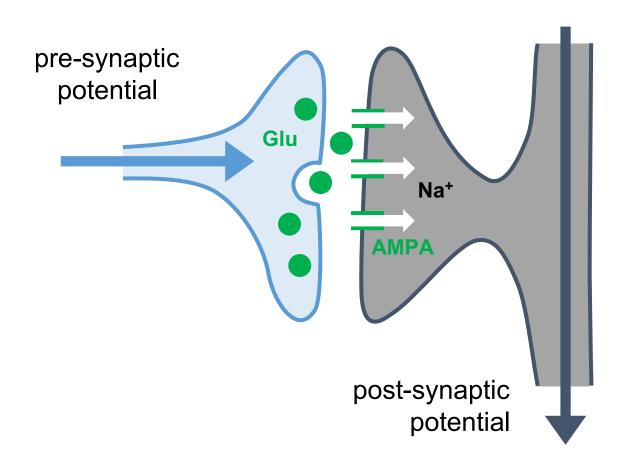
What kind of signals are generated in the brain

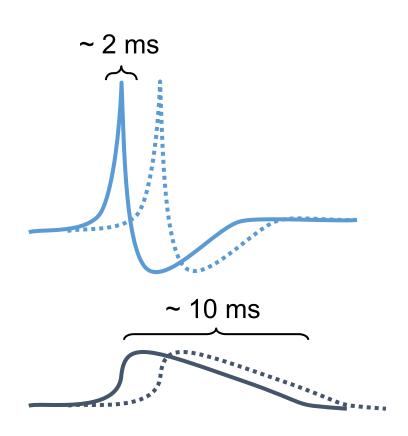
We measure the scalp potentials or field associated with post-synaptic potentials in pyramidal neurons

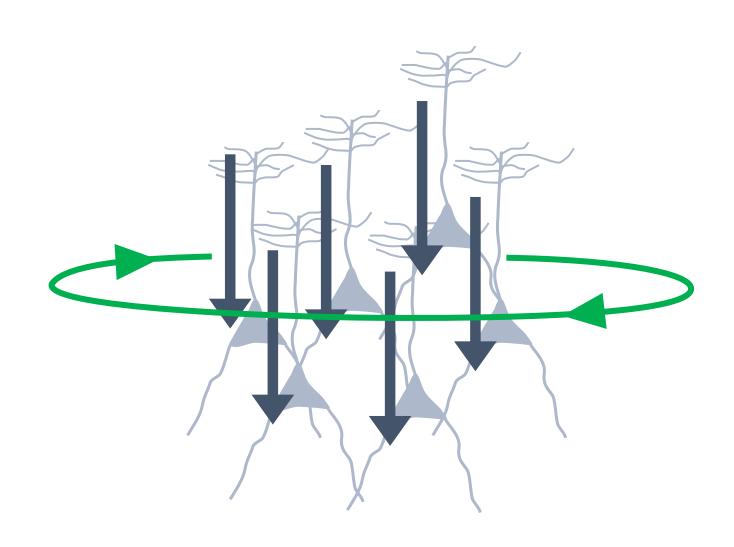
These PSPs represent the exitatory and inhibitory input that these neurons receive

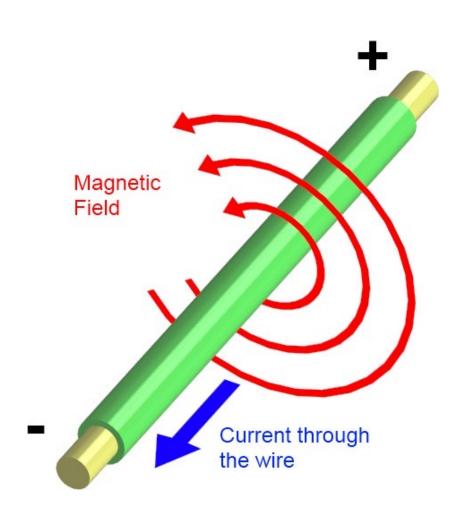
Usually we study this neuronal input following the presentation of a stimulus or following a cognitive event

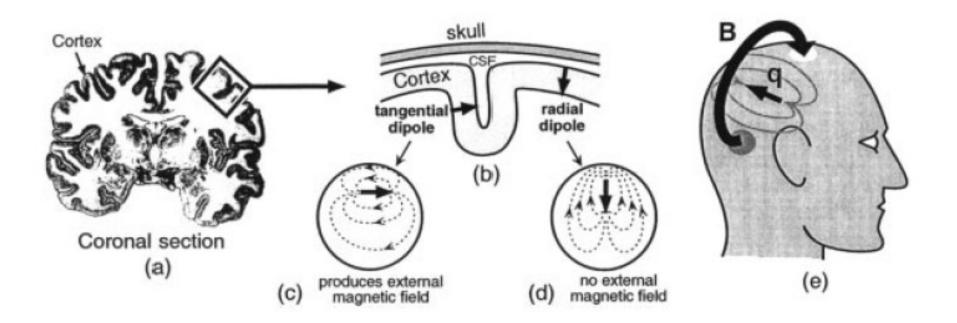




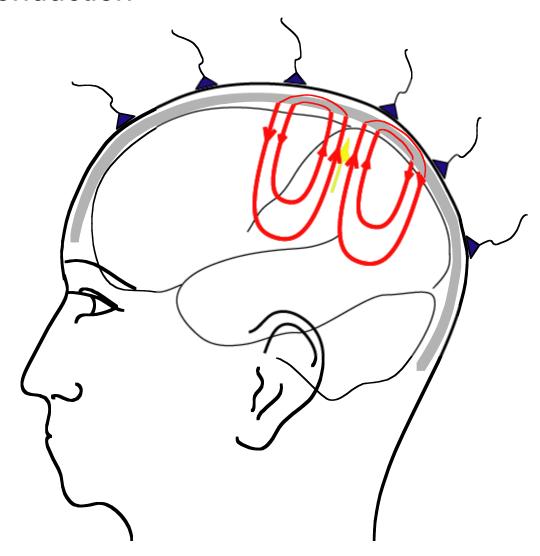




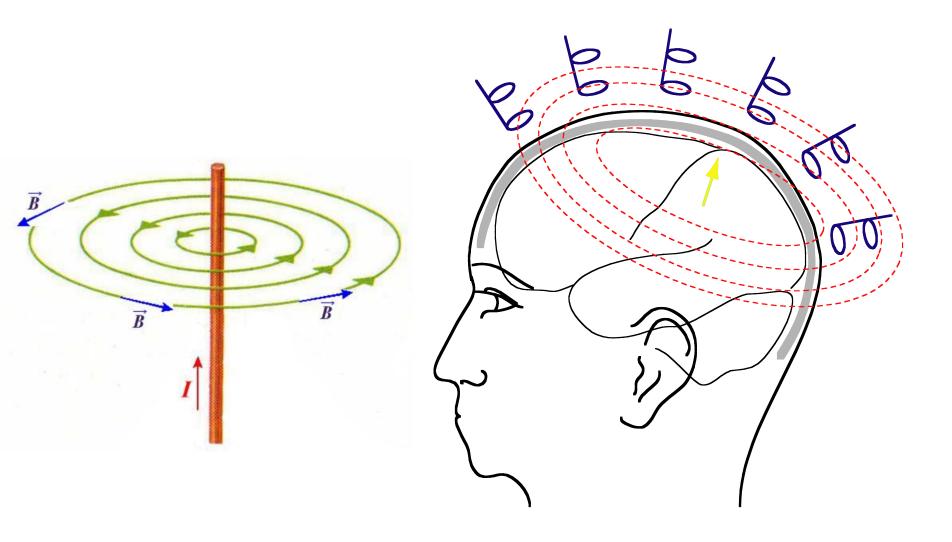




EEG volume conduction



Electric current → magnetic field



Talk outline

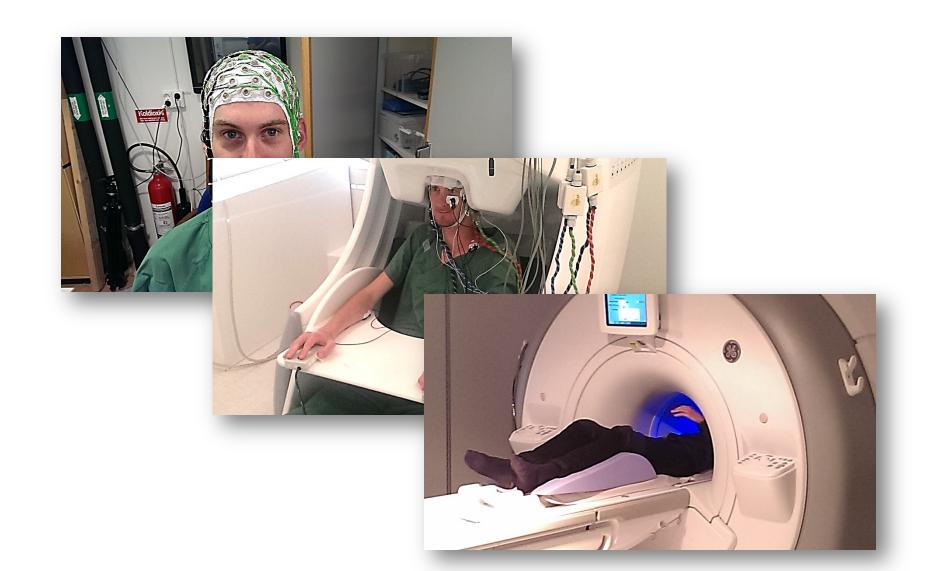
What kind of signals are generated in the brain

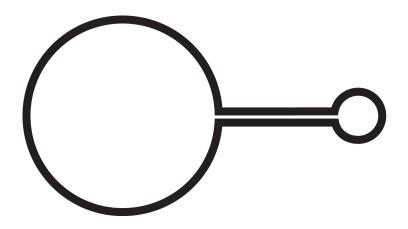
How do we record those signals

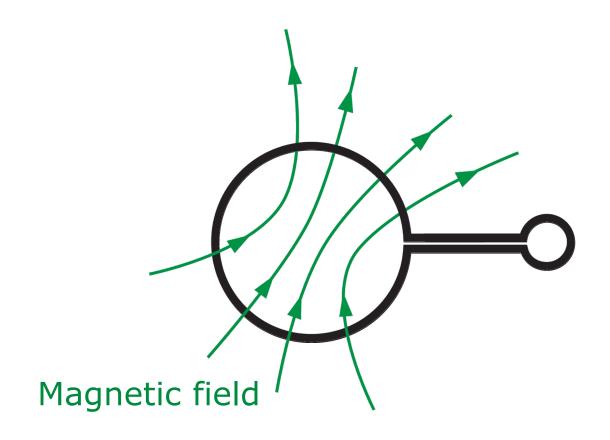
Analyzing those signals with FieldTrip

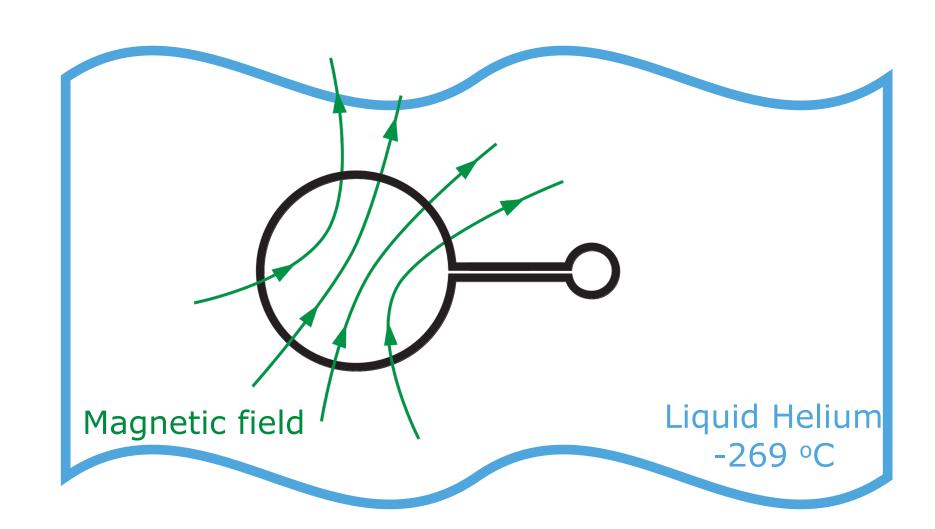
Background on the FieldTrip toolbox

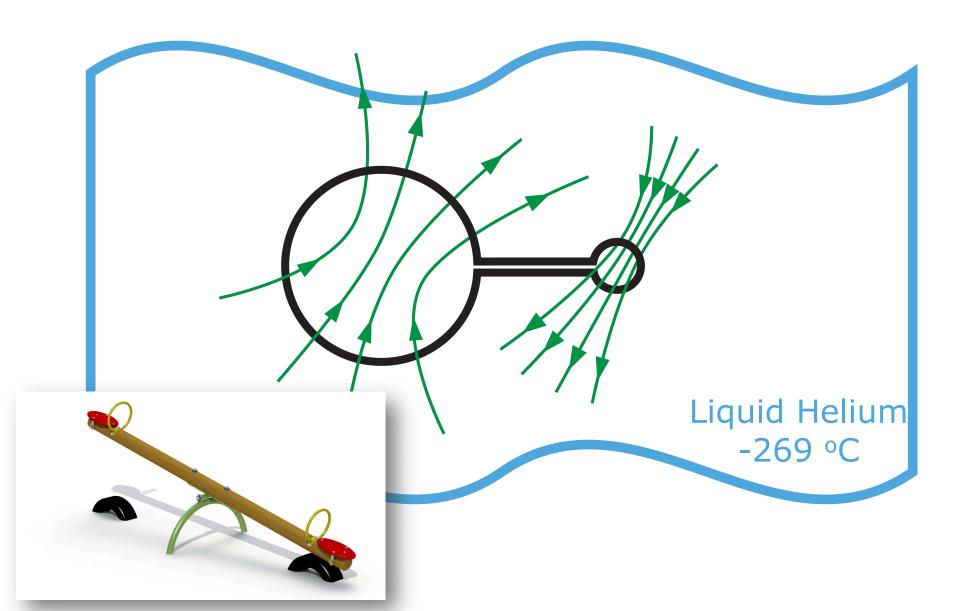
How do we record these signals from the brain

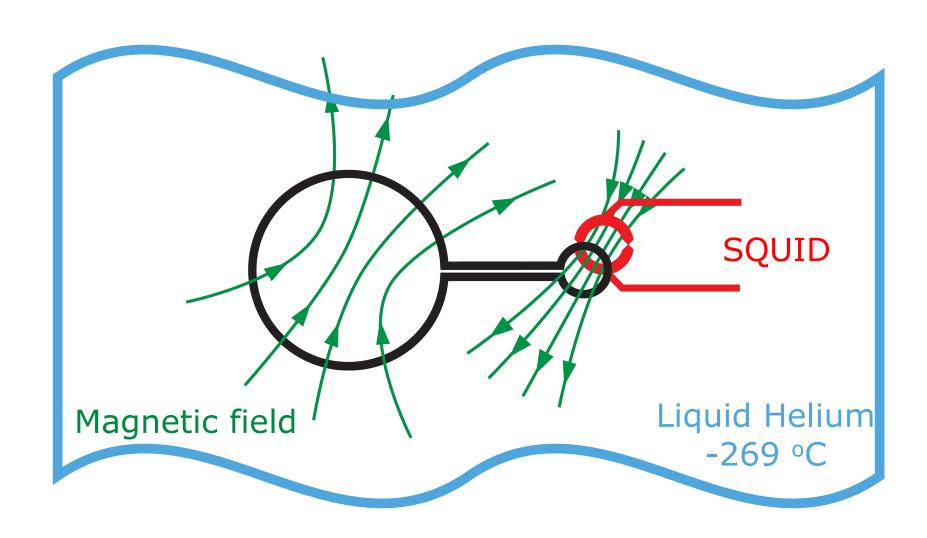




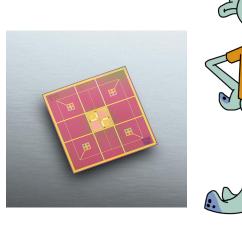


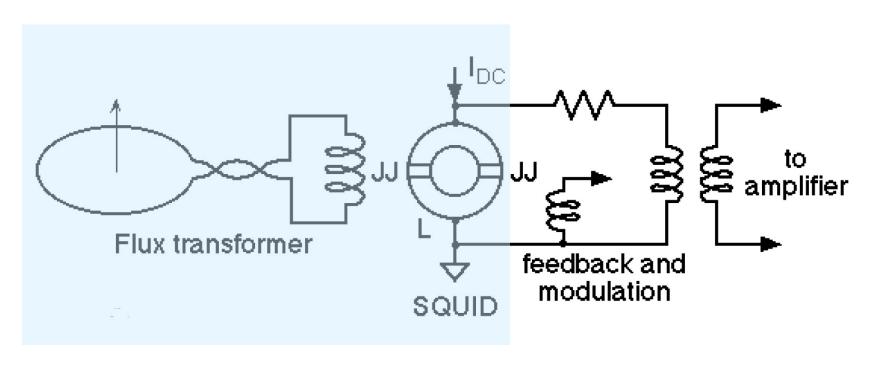






Magnetic field detectors Superconducting QUantum Interference Device





Magnetic field strength - compared

100	1.5 - 3 T	MRI systems
10-3	5 mT	typical refrigerator magnet
10-6	30-60 uT	earth's magnetic field
10-9	0.1 -10 nT	heliosphere
10-12	0.1 - 1.0 pT	spontaneous brain activity
10-15	10-100 fT	ERF differences

Technical challenges of MEG

Requires sensitive magnetic detectors

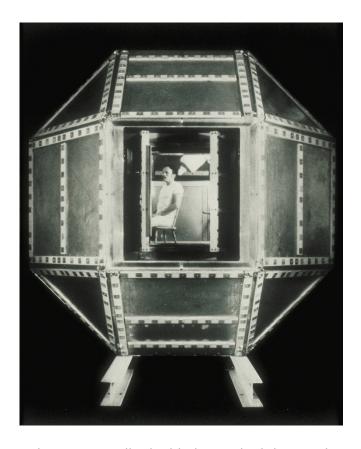
Deal with environmental noise

shielding

sensor design

reference sensors for noise subtraction

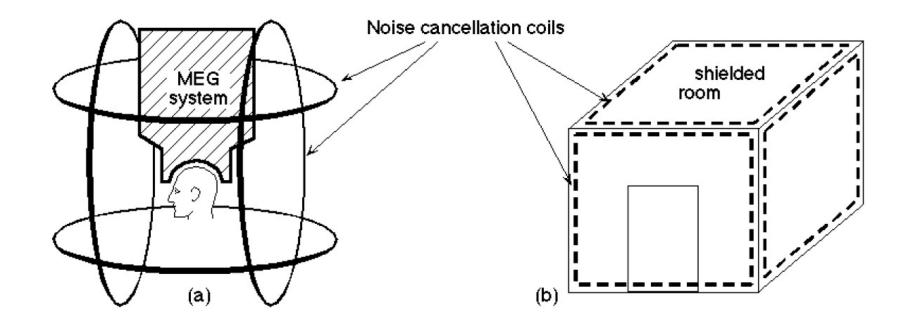
Shielding - passive

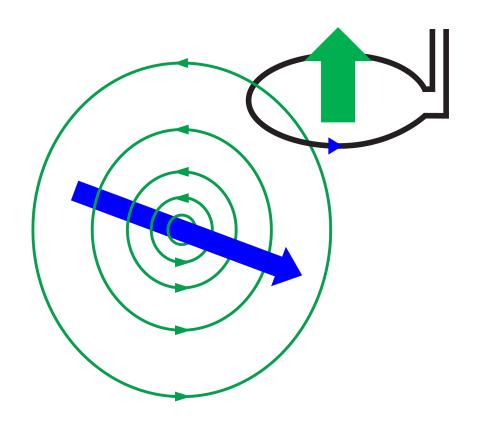


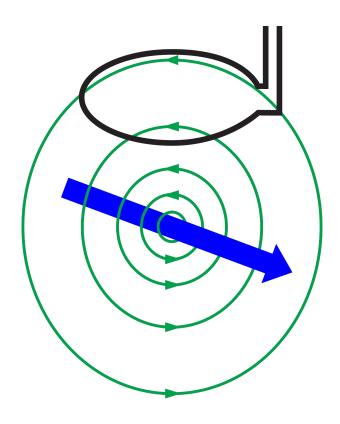
The magnetically shielded room built by David Cohen at MIT's Francis Bitter National Magnet Laboratory in 1969.

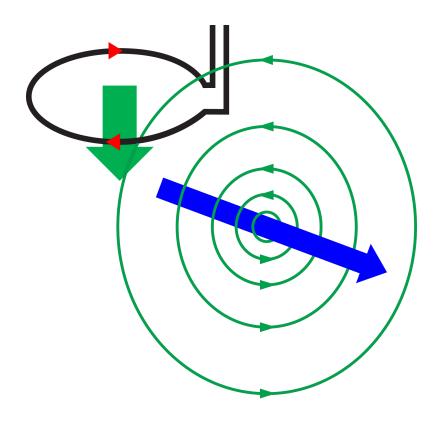


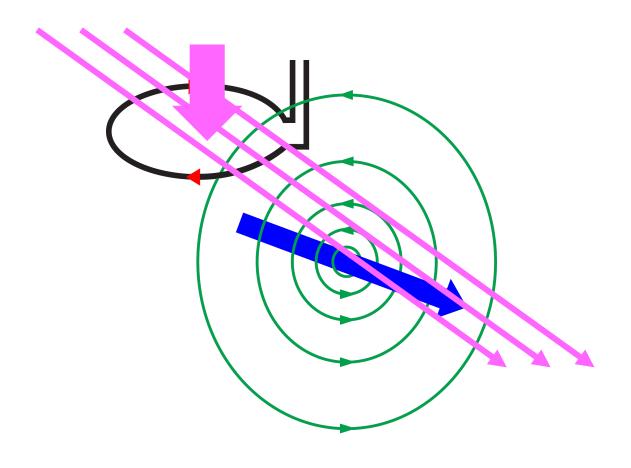
Shielding - active

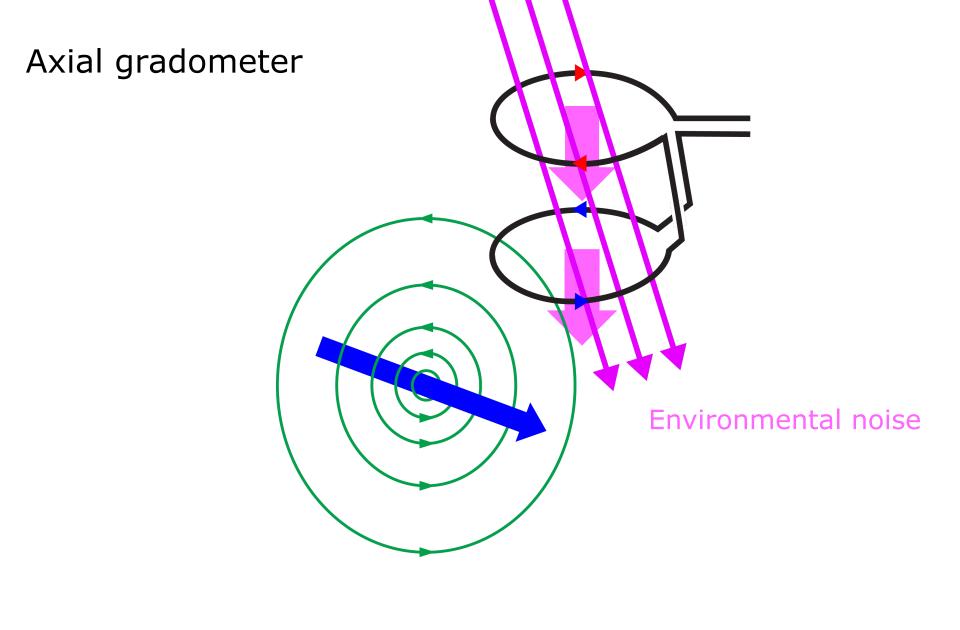




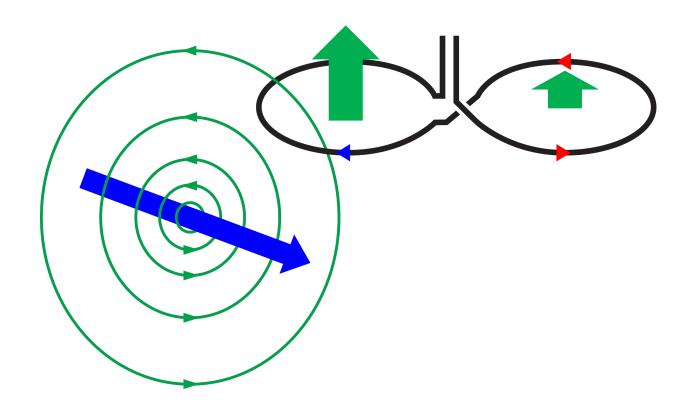


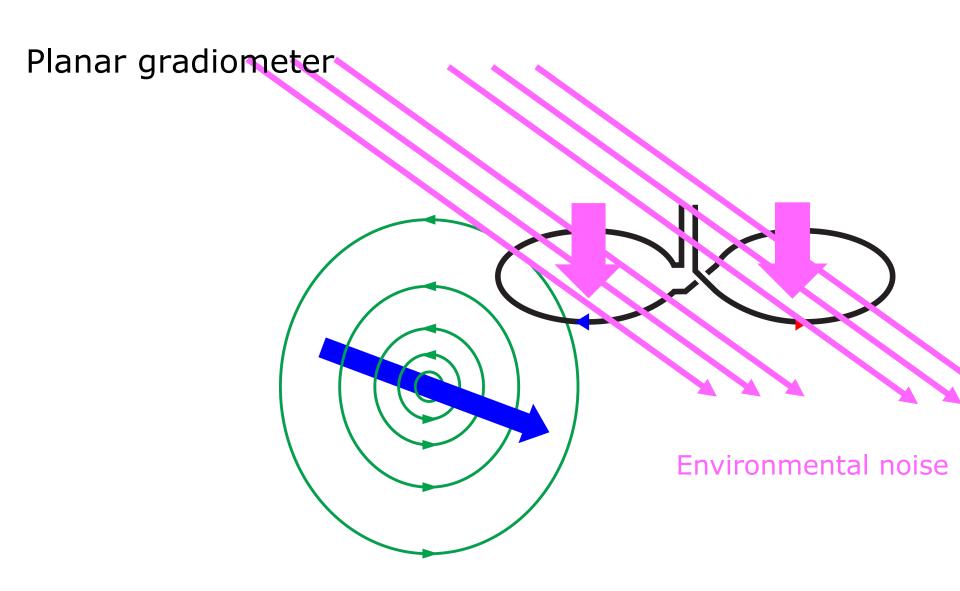




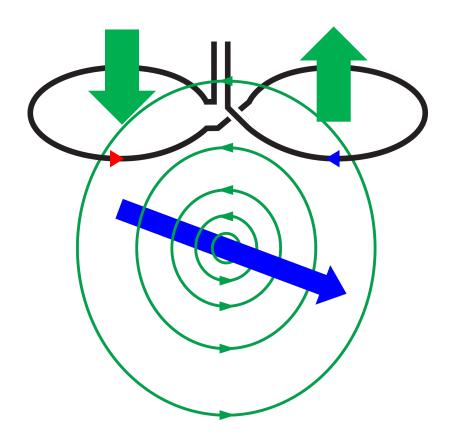


Planar gradiometer

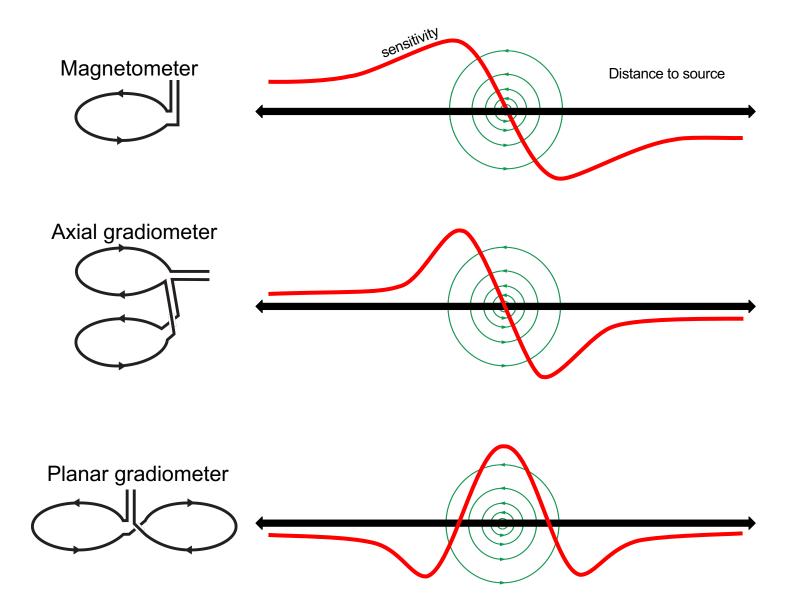


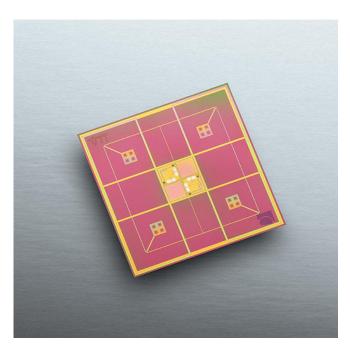


Planar gradiometer



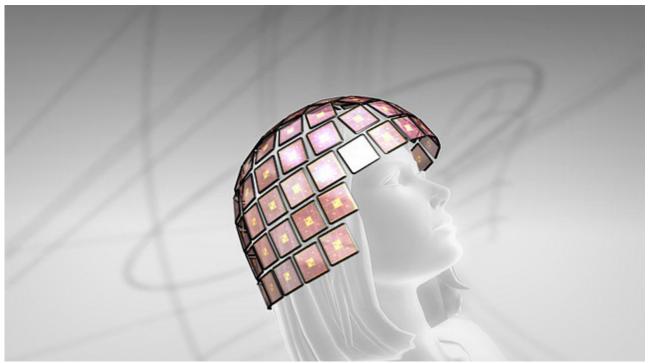
MEG sensor – sensitivity profile



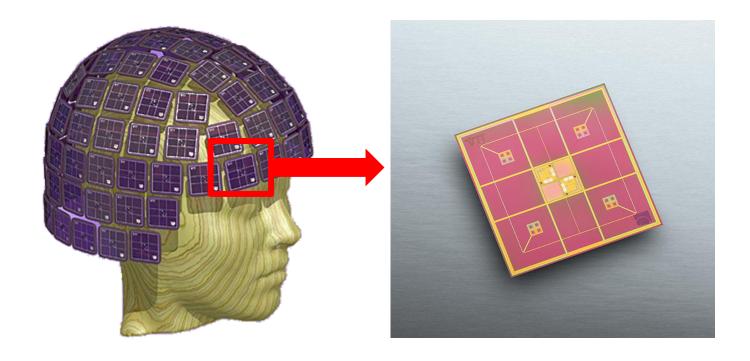


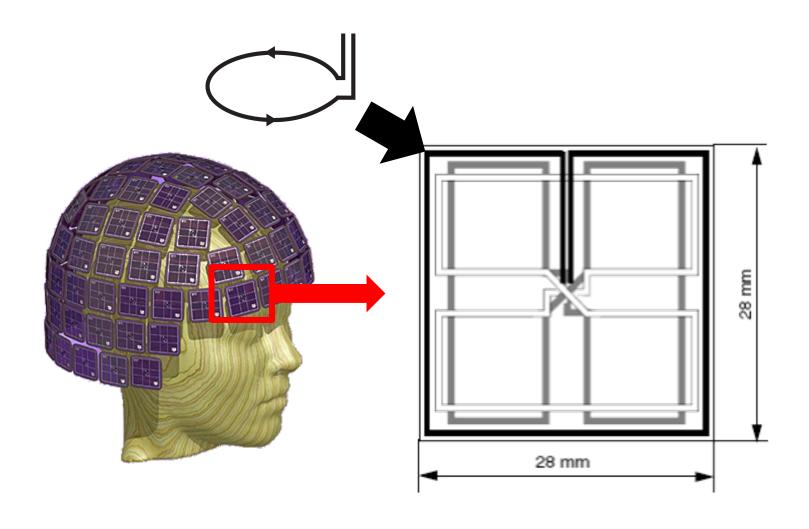
Neuromag/Elekta/Megin

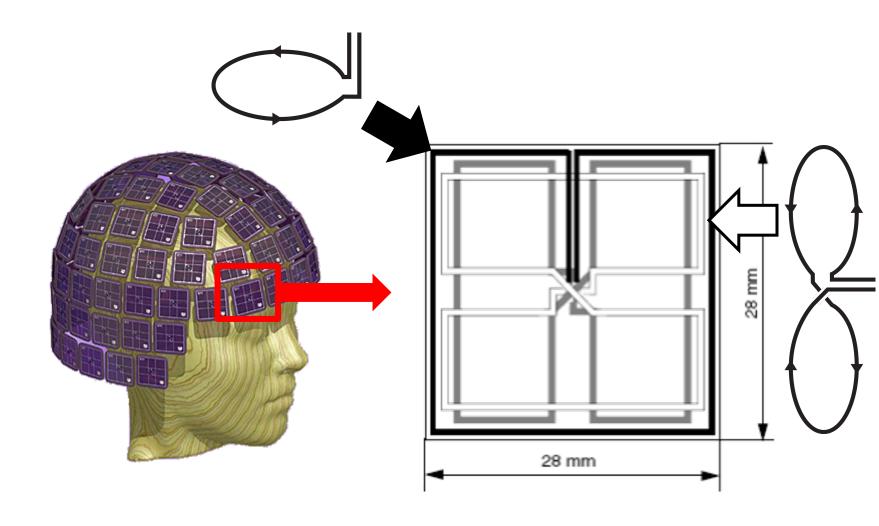
102 magnetometers204 planar gradiometers306 channels total



Neuromag/Elekta/Megin

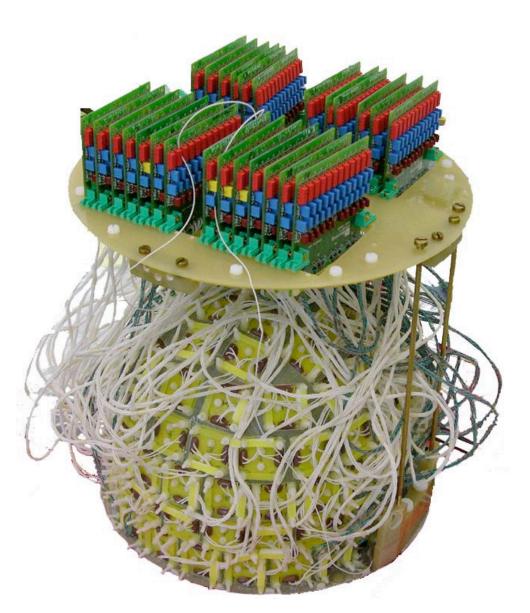




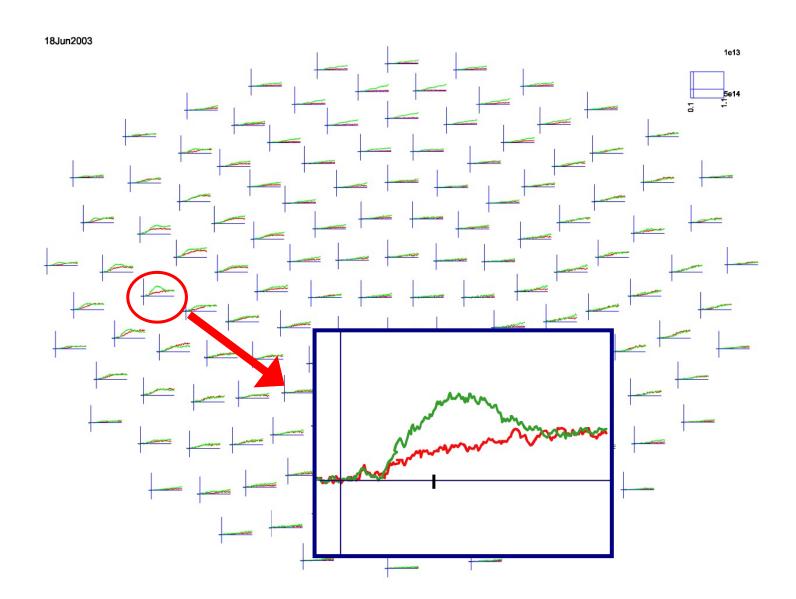


28 mm

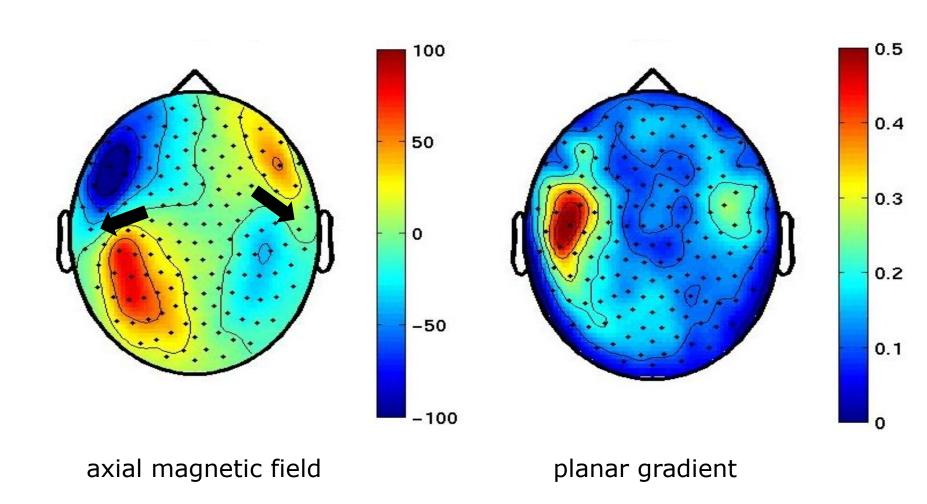




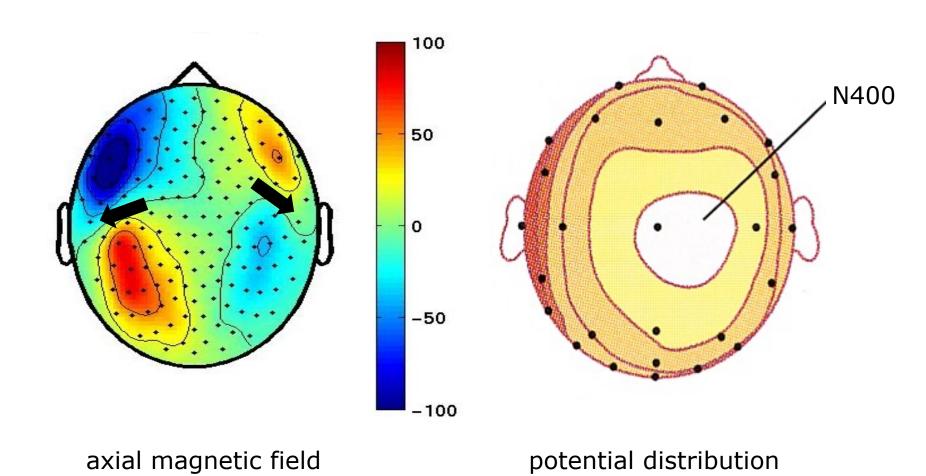
N400 response in MEG



N400 response - compared between MEG systems



N400 response - compared between MEG and EEG



LETTER

Moving magnetoencephalography towards real-world applications with a wearable system

Elena Boto¹*, Niall Holmes¹*, James Leggett¹*, Gillian Roberts¹*, Vishal Shah², Sofie S. Meyer^{3,4}, Leonardo Duque Muñoz³, Karen J. Mullinger^{1,5}, Tim M. Tierney³, Sven Bestmann^{3,6}, Gareth R. Barnes³§, Richard Bowtell¹§ & Matthew J. Brookes¹§

Imaging human brain function with techniques such as magnetoencephalography typically requires a subject to perform tasks while their head remains still within a restrictive scanner. This artificial environment makes the technique inaccessible to many people, and limits the experimental questions that can be addressed. For example, it has been difficult to apply neuroimaging to investigation of the neural substrates of cognitive development in babies and children, or to study processes in adults that require unconstrained head movement (such as spatial navigation). Here we describe a magnetoencephalography system that can be worn like a helmet, allowing free and natural movement during scanning. This is possible owing to the integration of quantum sensors^{2,3}, which do not rely on superconducting technology, with a system for nulling background magnetic fields. We demonstrate human electrophysiological measurement at millisecond resolution while subjects make natural movements, including head nodding,

stretching, drinking and playing a ball game. Our results compare well to those of the current state-of-the-art, even when subjects make large head movements. The system opens up new possibilities for scanning any subject or patient group, with myriad applications such as characterization of the neurodevelopmental connectome, imaging subjects moving naturally in a virtual environment and investigating the pathophysiology of movement disorders.

Magnetoencephalography¹ (MEG) allows direct imaging of human brain electrophysiology by measurement of magnetic fields generated at the scalp by neural currents. Mathematical analysis of those fields enables the generation of 3D images that show the formation and dissolution of brain networks in real time. MEG measurements of brain activity are currently made using an array of superconducting sensors placed around the head^{1,4}. These cryogenically cooled sensors have femtotesla (fT) sensitivity, which is needed to detect the weak magnetic fields produced by the brain. Unfortunately, the requirement

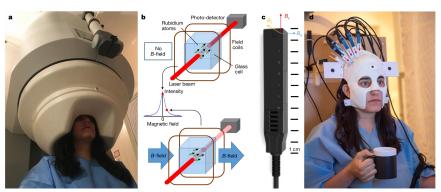


Figure 1 | A new generation of MEG system. a, A conventional 275-channel cryogenic MEG system. Weighing about 450 kg, the system is fixed and cumbersome and subjects must remain still relative to the fixed sensor array. b, Schematic illustration of zero-field resonance in an OPM sensor. Top, operation in zero-field, bottom, Larmor precession when an external field (*B*-field) impinges on the cell and the transmitted light intensity is reduced. c, A commercial OPM sensor made by QuSpin. The geometry used is illustrated by the coloured axes where *B*, is the radial

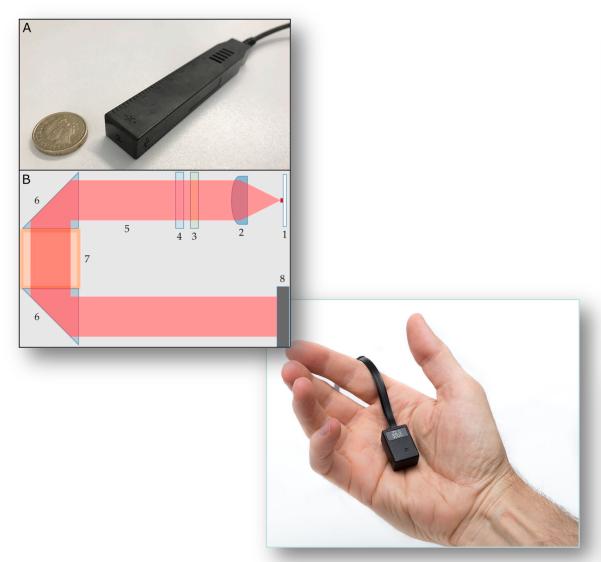
field component, B, the tangential field component and B, the direction along which the laser beam is oriented. A, Our prototype OPM-MEG system helmet. The helmet weighs 905 g and is customized so that the sensors (which in this prototype cover only the right sensorimotor cortex) are directly adjacent to the scalp surface. The subject is free to move their head. The measured radial field direction for the sensors is illustrated by the red arrows.

29 MARCH 2018 | VOL 555 | NATURE | 657

Sir Peter Mansfield Imaging Centre, School of Physics and Astronomy, University of Nottingham, University Park, Nottingham NG7 2RD, UK. ²QuSpin Inc., 331 South 104th Street, Suite 130, Louisville, Colorado 80027, USA. ³Wellcome Centre for Human Neuroimaging, UCL Institute of Neurology, University College London, 12 Queen Square, London WC1N 3BG, UK. ⁴Institute of Cognitive Neuroscience, University College London, 17-19 Queen Square, London WC1N 3RZ, UK. ⁴Centre for Human Brain Health, School of Psychology, University of Birmingham, Edgaston, Birmingham B15 2TT, UK. ⁴Sobell Department for Motor Neuroscience and Movement Disorders, UCL Institute of Neurology, University College London, Queen Square House, Queen Square, London WC1N 3BG, UK.

^{*}These authors contributed equally to this work \$These authors jointly supervised this work.









https://www.cercamagnetics.com

https://www.kernel.com https://fieldlineinc.com

https://quspin.com

https://youtu.be/6QizMOa4ZJM

Talk outline

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Background on the FieldTrip toolbox

M/EEG signal characteristics considered during analysis

timecourse of activity

-> ERP

spectral characteristics

-> power spectrum

temporal changes in power

-> time-frequency response (TFR)

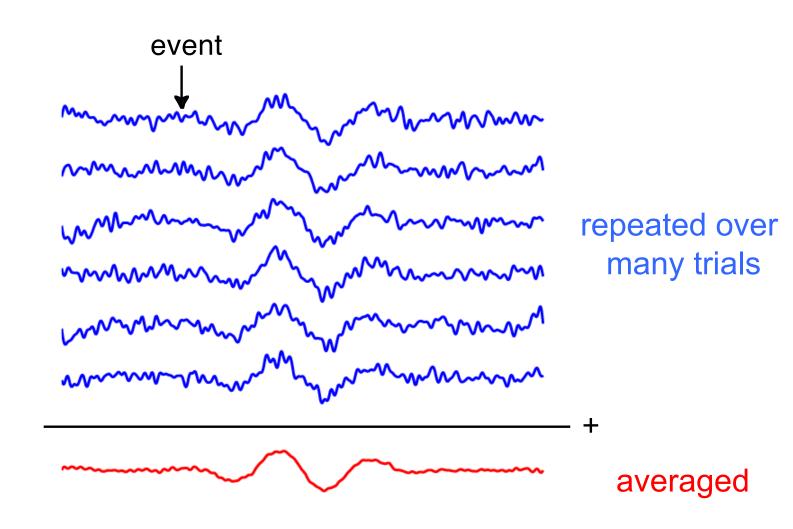
spatial distribution of activity over the head

-> source reconstruction

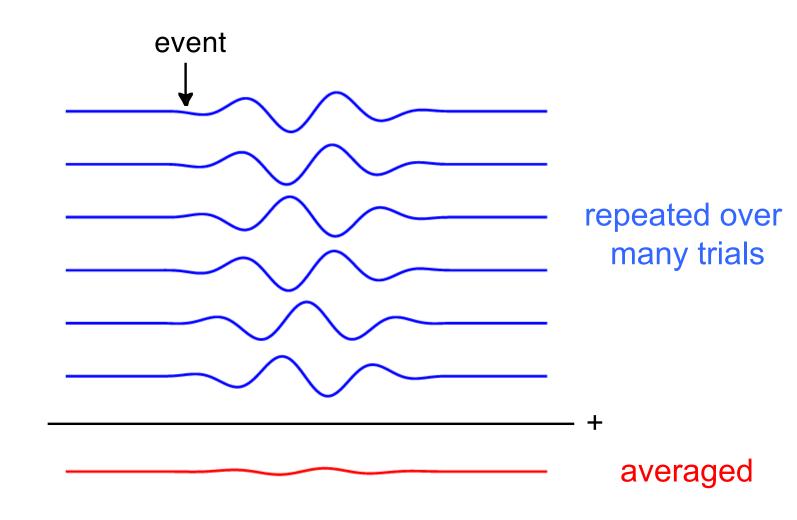
Evoked activity

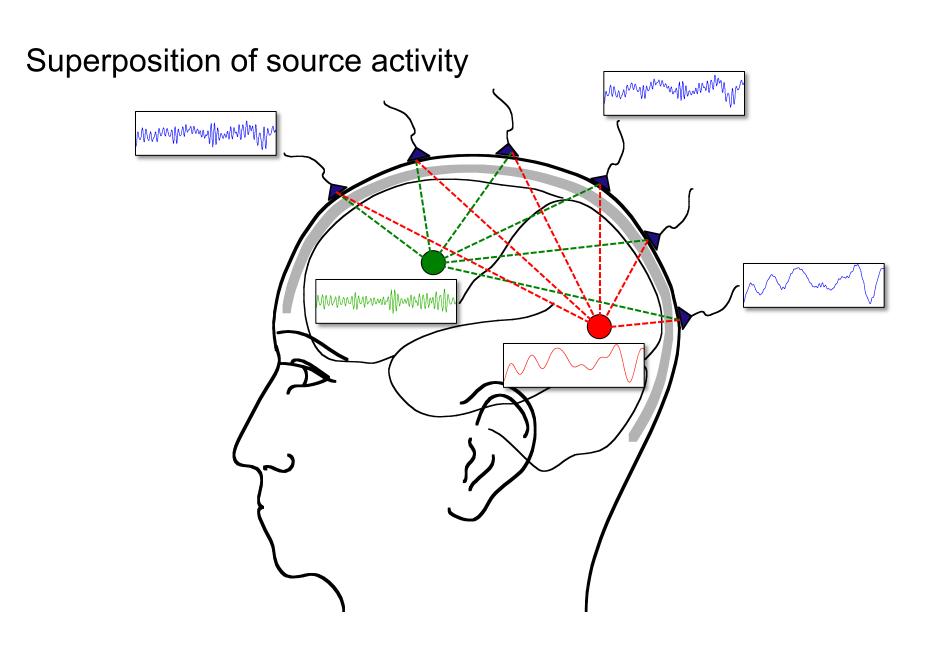


Evoked activity



Induced activity





Separating activity of sources

Use the temporal aspects of the data at the channel level

ERF latencies

ERF difference waves

Filtering the time-series

Spectral decomposition

Use the spatial aspects of the data

Volume conduction model of head

Estimate source model parameters

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Some FieldTrip basics



the "cfg" argument is a contiguration structure, e.g.

```
cfg.channel = {'C3', C4', 'F3', 'F4'}
cfg.foilim = [1 70]
```

FieldTrip v.s. default Matlab

dataout = functionname(cfg, datain, ...)

cfg.key1 = value1 cfg.key2 = value2

dataout = functionname(datain, key1, value1, ...)

Using functions in an analysis protocol

ft_preprocessing

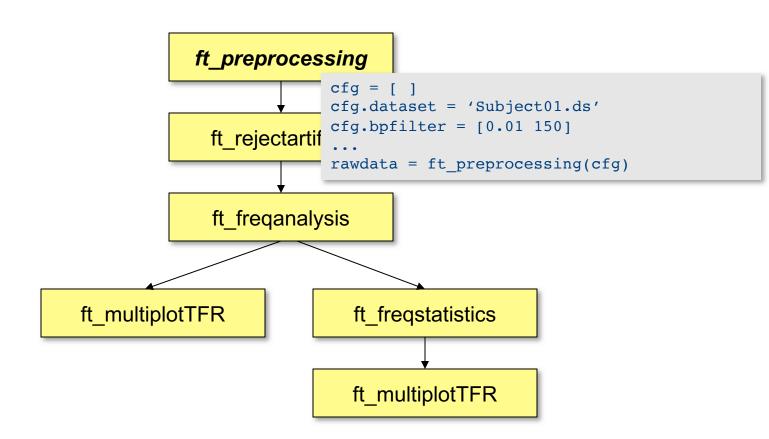
FT_PREPROCESSING reads MEG and/or EEG data according to user-specified trials and applies several user-specified preprocessing steps to the signals.

```
Use as
  [data] = ft_preprocessing(cfg)
or
  [data] = ft_preprocessing(cfg, data)
```

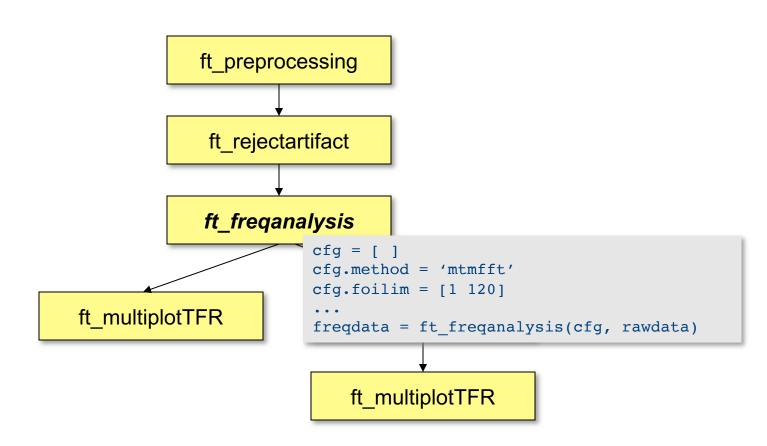
The first input argument "cfg" is the configuration structure, which contains all details for the dataset filenames, trials and the preprocessing options. You can only do preprocessing after defining the segments of data to be read from the file (i.e. the trials), which is for example done based on the occurence of a trigger in the data.

• • •

Using functions in an analysis protocol



Using functions in an analysis protocol



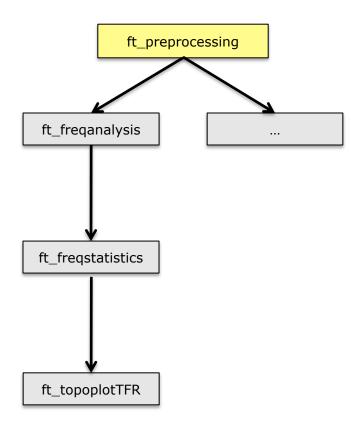
Raw data structure

```
rawData =
    label: {151x1 cell}
    trial: {1x80 cell}
    time: {1x80 cell}
    fsample: 300
    hdr: [1x1 struct]
    cfg: [1x1 struct]
```

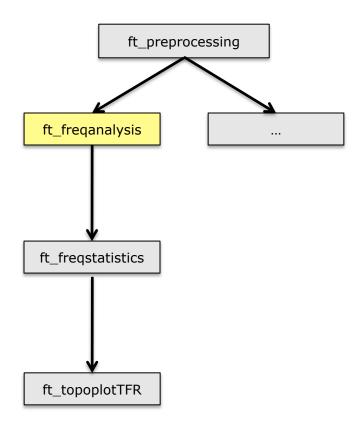
Event related response

```
timelockData =
    label: {151x1 cell}
    avg: [151x900 double]
    var: [151x900 double]
    time: [1x900 double]
    dimord: 'chan_time'
    cfg: [1x1 struct]
```

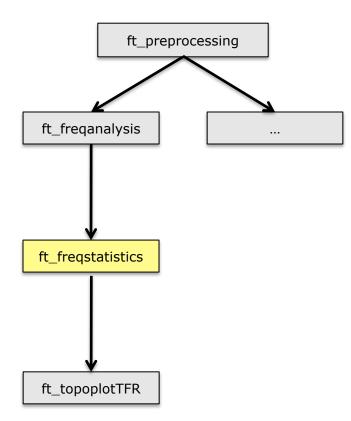
```
cfg = []
cfg.dataset = 'Subject01.ds'
cfg.bpfilter = [0.01 150]
rawdata = ft preprocessing(cfg)
```

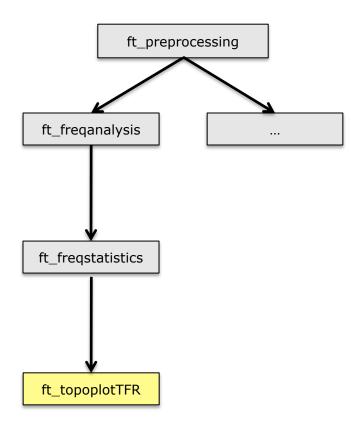


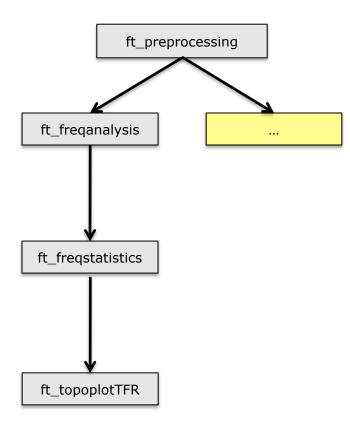
```
cfg = []
cfg.method = 'mtmfft'
cfg.foilim = [1 120]
freqdata = ft freqanalysis(cfq, rawdata)
```



```
cfq = []
cfg.method = 'montecarlo'
cfq.statistic = 'indepsamplesT'
cfg.design = [1 2 1 2 2 1 2 1 1 2 ...]
freqstat = ft freqstatistics(cfg, freqdata)
```







```
subj = {'S01.ds', 'S02.ds', ...}
trig = [1 \ 3 \ 7 \ 9]
for s=1:nsubj
for c=1:ncond
 cfg = []
  cfg.dataset = subj{s}
  cfg.trigger = trig(c)
  rawdata{s,c} = ft preprocessing(cfg)
  cfg = []
  cfg.method = 'mtmfft'
  cfg.foilim = [1 120]
  freqdata{s,c} = ft freqanalysis(cfg, rawdata{s,c})
end
end
```

```
subj = {'S01.ds', 'S02.ds', ...}
trig = [1 \ 3 \ 7 \ 9]
for s=1:nsubj
for c=1:ncond
 cfg = []
  cfg.dataset = subj{s}
  cfg.trigger = trig(c)
  rawdata = ft preprocessing(cfg)
  filename = sprintf('raw%s_%d.mat', subj{s}, trig(c));
  save(filename, 'rawdata')
end
end
```

Example use in distributed computing

```
subj = {'S01.ds', 'S02.ds', ...}
trig = [1 \ 3 \ 7 \ 9]
for s=1:nsubj
for c=1:ncond
 cfgA\{s,c\} = []
 cfgA{s,c}.dataset = subj{s}
 cfgA{s,c}.trigger = trig(c)
 cfgA{s,c}.outputfile = sprintf('raw%s %d.mat', subj{s}, trig(c))
 cfgB\{s,c\} = []
 cfgB{s,c}.dataset = subj{s}
 cfgB{s,c}.trigger = trig(c)
  cfgB{s,c}.inputfile = sprintf('raw%s %d.mat', subj{s}, trig(c));
 cfgB{s,c}.outputfile = sprintf('freq%s %d.mat', subj{s}, trig(c));
end
end
dfeval(@ft_preprocessing, cfgA)
dfeval(@ft freqanalysis, cfgB)
```

Example use in distributed computing

```
subj = {'S01.ds', 'S02.ds', ...}
trig = [1 \ 3 \ 7 \ 9]
for s=1:nsubj
for c=1:ncond
 cfgA\{s,c\} = []
 cfgA{s,c}.dataset = subj{s}
 cfgA{s,c}.trigger = trig(c)
 cfgA{s,c}.outputfile = sprintf('raw%s %d.mat', subj{s}, trig(c))
 cfgB\{s,c\} = []
 cfgB{s,c}.dataset = subj{s}
 cfgB{s,c}.trigger = trig(c)
  cfgB{s,c}.inputfile = sprintf('raw%s %d.mat', subj{s}, trig(c));
 cfgB{s,c}.outputfile = sprintf('freq%s %d.mat', subj{s}, trig(c));
end
end
qsubcellfun(@ft_preprocessing, cfgA)
qsubcellfun(@ft freqanalysis, cfgB)
```

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FieldTrip is a toolbox

the data and the separate functions are in your hands

the scripts depend on the data properties, your computer and on your programming skills and style

scripts correspond to analysis protocols

scripts can be reviewed by supervisors scripts are often shared with colleagues scripts can be published/released

Finding your way around in the FieldTrip toolbox

Matlab

help functionname edit functionname

Website

http://www.fieldtriptoolbox.org

Email discussion list

Expertise in your local group